

1 **Creating movable interfaces by micro-powder injection moulding**

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8 9 **Abstract**

10 This paper presents a novel in-situ technique to produce articulated components with high-
11 precision, micro-scale movable interfaces by micro-powder injection moulding (μ PIM). The presented
12 process route is based on the use of micro-scale sacrificial layer between the movable subcomponents
13 which is eliminated during the debinding step, creating a dimensionally-controlled, micro-scale mobile
14 interface. The fabrication technique combines the advantages of micro-powder overmoulding, catalytic
15 debinding and sintering. The demonstrated example was a finger bone prosthesis joint consisting of two
16 sub-components with an interface between components of 200 μ m in size. The geometries of the sub-
17 components were designed such that they are inseparable throughout the process whilst allowing them to
18 move relative to each other after the debinding stage. The components produced showed the feasibility of
19 the process route to produce readily-assembled meso-, and potentially micro-, scale articulated systems.

20
21 **Keywords:** Micro-powder injection moulding, Metal injection moulding, Micro-cavities, Micro-joints,
22 Microfabrication, Three-dimensional

23 24 **1. Introduction**

25 Small-scale joints are becoming crucial to the development of the next generation of meso-scale
26 devices. Articulated systems with movable interfaces are particularly important for meso- and micro-scale
27 components. Examples include finger bone replacements, known as phalangeal prostheses, which have
28 component sizes in the order of few millimetres and tolerances in the order of hundreds of microns, such
29 as those tested by Field (2008) and Middleton et al. (2011). Another application for micro-scale

30 components with moving joints are ‘micro-engines’, which are micro-scale, power generation devices,
31 currently under consideration as replacements for batteries in consumer portable devices. Typical micro-
32 engines have component sizes in the order of millimetres and tolerances in the order of tens of microns,
33 such as the examples demonstrated by Hassanin and Jiang (2010) and Zhu et al. (2010). ‘Micro-
34 manipulators’ is another example of micro-scale devices with articulated components, which are used to
35 remove, manipulate or deliver micro-scale elements, for example cells in medical applications, which
36 have different sizes and tolerances in the order of few microns to tens of microns. Kim et al. (2008) have
37 presented demonstrations of such systems.

38 In spite of the growing applications of metallic components with movable structures, current
39 processing routes pose several constraints on the design and manufacturing routes of such complex
40 structures. Such constraints result in considerable increase in manufacturing time and cost.

41 Whilst fabrication processes for the construction of multiple rigid bodies and their connecting
42 joints - known as kinematic chains - are well characterized at the conventional (macro-) scale, at the
43 micro-scale processes are still in their infancy. This is due to a number of challenges, the most significant
44 of which are: a. limitations on the geometry of fabricable structures, b. material selection limitations, c.
45 assembly challenges, d. powder-based fabrication challenges and e. mass manufacturability.

46 In terms of geometry limitations, joints possess usually one, or exceptionally two, degrees of
47 translational or rotational freedom, a limitation imposed by the variants of ‘axial’ processes (normally
48 lithography or cutting) used in their fabrication. This is evident in the examples available in the literature,
49 such as movable, silicon-based micro-structures produced by Fan et al. (1988) for sensors and actuators,
50 movable microfluidic elements demonstrated by Ling and Lian (2007) using SU-8 fabrication, silicon-
51 based, micro-hinges produced by Pister et al. (1992) and movable micro-gears fabricated from SU-8 by
52 Seidemann et al. (2002).

53 The second limitation imposed on meso- and micro-scale movable structures is materials
54 selection. Such structures are severely restricted in terms of possible materials. As illustrated above,
55 materials used for such applications are currently usually either silicon or SU8 (an epoxy-based
56 photoresist). Such materials are notable for their poor wear resistance in moving parts, as illustrated by
57 both Waits et al (2007) and Hergert et al. (2010) in two independent experiments about wear damages
58 induced in micro-scale ball bearings produced by silicon fabrication techniques.

59 Assembling relatively small structures is another major challenge, because such assemblies are
60 currently done by post-processing techniques and, therefore, require accurate alignment and tolerance
61 checking. As mentioned above, currently, in-situ alignment has only been achieved with lithographic
62 techniques using materials of limited mechanical performance, notably silicon and SU8. A number of
63 such assembly techniques have been reviewed by Leong et al. (2010) for micro-scale components. For
64 relatively-larger, meso-scale systems, post-processing assembly is usually implemented, such as a press-
65 fit mechanism, as illustrated by Koch and Sandoz (1994) for metal finger joint prosthesis.

66 To overcome the material and geometrical limitations of silicon and SU8, some recent research
67 has started to investigate the use of powder-based fabrication of micro-scale joints. Additive
68 manufacturing, for example, has been investigated by Yang et al. (2011) for manufacturing
69 conventionally-sized metal joints by laser selective melting. However, the process is comparatively slow
70 and not optimized for micro-scale applications. On the micro-scale, recent work has attempted to produce
71 micro-scale moving joints using powder-based ceramics. The idea was to co-sinter two components made
72 of different materials in order to achieve the clearance required to facilitate motion by difference in
73 volumetric shrinkage of the two materials. Demonstrations have been made by Piotter et al. (2010a and
74 2010b) and Ruh et al. (2008 and 2010) using powder injection moulding. Such a procedure requires
75 careful adjustment of process conditions to achieve the exact shrinkage in subcomponents, such that a
76 movable clearance is achieved.

77 The challenge of mass manufacturability of assembled structures is associated with a number of
78 obstacles. Firstly, post-processing assembly extends the time and cost of the process chain to ensure
79 accurate alignment and movement, especially if the microfabrication process itself is relatively slow.
80 Secondly, in case of in-situ assembly using silicon etching or similar techniques, the process is not mature
81 enough for mass-fabrication.

82 This paper presents a technique using metal powders to produce moving components with
83 dimensionally controlled micro-scale interfaces by μ PIM as a high-volume microfabrication process. A
84 review of the μ PIM and its applications for micro-scale components is available in the literature (Attia
85 and Alcock, 2011a). The following sections detail the proposed methodology through a demonstrator, and
86 the discussion will assess the capability of the proposed technique to overcome the five challenges
87 highlighted above.

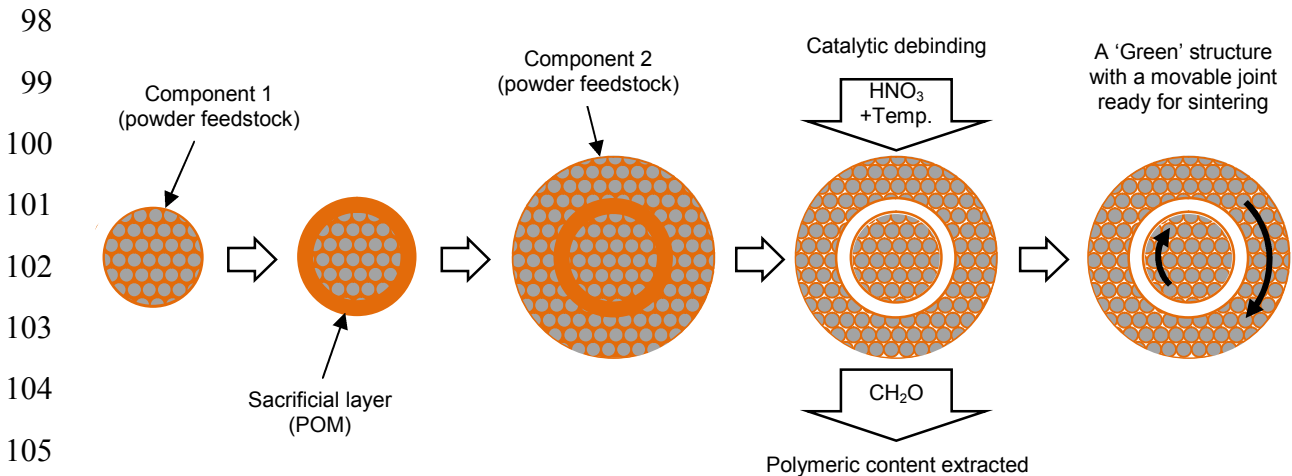
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89 2. Experimental

90 2.1 Methodology

91 Here we report on a strategy by which articulated architectures with micro-scale 3-D cavities can
92 be fabricated using a lost-core approach. The authors have previously demonstrated the possibility of
93 producing dimensionally controlled, enclosed micro-cavities by sequential powder over-moulding of
94 metals (Attia and Alcock, 2012) and ceramics (Attia and Alcock, 2011b).

95 The hypothesis explored here was that a further development of such a methodology could be
96 used to create “open” cavities/spaces between two or more components, such that the components could
97 move relative to each other. Figure 1 presents a schematic illustration of the technique.



106 **Fig. 1.** A schematic illustration of catalytic debinding with a sacrificial core.

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108 Briefly, one component is fabricated out of a metallic feedstock by μPIM . A micro-scale
109 polymeric sacrificial layer is then overmoulded in the position relative to the first component at which a
110 cavity is eventually required. The second component, made of powder feedstock, is overmoulded on top
111 of the polymeric layer, ensuring, in the design and fabrication steps, that it has no contact points with the
112 first component.

113 The resulting rigid structure is then catalytically debound, where nitric acid vapour is used to
114 hydrolyse the POM of both the sacrificial layer and the components' binder into formaldehyde, which is
115 extracted during the process. The resulting space allows for a relative motion between the two
116 components, which are subsequently sintered for full densification.

117 The powder feedstock consists of the metallic powder, mixed with a catalytically debindable
118 polymer, in this case polyoxymethylene (POM). The sacrificial layer is made of the same polymer so that
119 both the polymeric content of the powder feedstock and the core could be simultaneously eliminated
120 during catalytic debinding.

121 Stainless steel 316L was the material selected for this experiment for two main reasons. Firstly,
122 stainless steel 316L is commercially available as a readily mixed feedstock consisting of powder particles
123 with relatively small mean sizes (4-5 μm), which makes it suitable for micro-moulding applications.
124 Using a commercial grade of feedstock makes it possible to assess the viability and consistency of the
125 proposed process independent of factors related to mixing special medical grade powders.

126 The second reason for using 316L is that it is one of the most widely used materials for
127 replicating conventional and micro-scale features by metal injection moulding (MIM). There is a
128 considerable amount of previous work that looked into investigating different aspects of the powder
129 injection moulding of 316L.

130 For example, with regard to mixing and characterising 316L feedstock, Liu et al. (2005) used
131 316L to assess the effects of powder loading and mixing conditions on feedstock homogeneity and shape
132 retention of micro-moulded features. Abolhasani and Muhamad (2010) developed a new 316L feedstock
133 for MIM based on starch as a binding material. Samanta et al. (2011) characterised the thermo-physical
134 properties of an in-house mixture of a 316L feedstock for MIM. Kong et al. (2012) demonstrated a
135 procedure to determine the optimal powder loadings for 316L stainless steel feedstock for micro-powder
136 injection moulding.

137 With regard to process development, Loh et al. (2003) used 316L feedstock to replicate
138 microstructure arrays with aspect ratios up to 2 using silicon inserts. Their work focused on the effect of
139 process conditions on replication quality of micro-scale features.

140 Debinding 316L has also been investigated in a number of experiments. For example, Omar et al.
141 (2003) demonstrated a two-stage rapid debinding technique combining solvent and thermal debinding of
142 316L feedstock. Li et al. (2003) compared the binder removal rate in vacuum and hydrogen environments
143 during thermal debinding of 316L. The effect of thermal debinding of 316L feedstock on surface
144 roughness of moulded components was also studied by Liu et al. (2007).

145 With regard to using 316L in variant MIM processes, Rota (2002) demonstrated the principle of
146 sinter-bonding of two 316L components produced by micro-metal injection moulding. Nishiyabu et al.
147 (2007) demonstrated a lost-core technique to produce microstructured 316L components by micro-
148 injection moulding. In addition, Imgrund et al. (2008) co-injection moulded 316L and 17-4PH to produce
149 magnetic-nonmagnetic bimetals by micro-MIM. 316L powder was also used by Manonukul et al. (2010)
150 to demonstrate a technique to produce metal foam by metal injection moulding using a powder space
151 holder.

152 With regard to properties of sintered 316L components, Castro et al. (2003) studied the
153 mechanical properties and pitting corrosion behaviour of 316L. Tay et al. (2005) investigated the effect of
154 sintering conditions on the surface roughness of microstructured components produced by injection
155 moulding of 316L. Huang and Hsu (2009) compared the effect of three backbone polymers on the
156 mechanical properties of 316L specimens produced by MIM, showing that HDPE performs best in terms
157 of both the flow stability and the MIM compact quality. Rafi Raza et al. (2012) studied the effects of
158 cooling rate on mechanical properties and corrosion resistance of vacuum sintered powder injection
159 moulded 316L stainless steel. They showed that higher cooling rates improved mechanical properties and
160 corrosion resistance compared to lower cooling rates.

161 Catalytic debinding was particularly selected for the process route presented in this paper,
162 because it is a direct solid-gas transition process that takes place below the T_g of the polymer. The process,
163 therefore, results in higher dimensional accuracy, tighter tolerances and better surface finish relative to
164 other debinding techniques (German, 1998). Such characteristics make catalytic debinding an attractive
165 process for applications requiring dimensional accuracy and tight tolerances. A recent market study has
166 showed that 21% of the MIM industry currently relies on catalytic debinding (German and Atre, 2013)

167 Catalytic debinding of 316L has been investigated in several experiments. Examples include the
168 work reported by Fu et al. (2004), where the use of uMIM to produce 316L microstructural arrays of
169 high-aspect ratios was investigated in a process that involved catalytic debinding. The same group also
170 studied the effect of moulding process parameters on the filling quality of the array microstructures (Fu et
171 al., 2005a) and used catalytic debinding to produce microstructural arrays made of 316L with good shape
172 retention (Fu et al., 2005b).

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174 *2.2 Experimental procedure*

175 *2.2.1 Structure design and operation*

176 The application presented in the paper is a finger bone replacements, which has component sizes
177 in the order of few millimetres and tolerances in the order of hundreds of micrometres. Similar prosthesis
178 are usually fabricated as separate components and assembled by post processing as previously discussed
179 in the introduction.

180 The structure selected for illustrating the process chain is for a finger-bone prosthesis, which was
181 selected as a demonstrator for the proposed process for a number of reasons:

- 182 i. The structure consists of moving components with micro-scale tolerances in the order of hundreds of
183 microns.
- 184 ii. The geometries of the subcomponents are three-dimensional in nature, with free-form surfaces
185 within the joint itself, which makes them unsuitable for conventional 2½-D manufacturing
186 processes.
- 187 iii. The structure requires assembling the two-subcomponents, which is done as a post-processing step
188 in state-of-the-art designs, and which this work attempts to do it in-situ (more details about the
189 design of the assembly mechanism in the description of figure 2 below).
- 190 iv. Such a component poses special material requirements in terms of mechanical properties and
191 biocompatibility, which could be fulfilled with powder technology.

192 The process presented in Figure 1 was implemented to fabricate a readily assembled prosthesis
193 consisting of a cylinder and socket structure. The cylinder and socket subcomponents will be referred to
194 as “part 1” and “part 2”, respectively, throughout the text.

195 Figure 2 shows a CAD illustration of the structure with the main dimensions. The structure
196 consists of two sub-components joined in a cylinder-and-socket format with a one-degree-of-freedom
197 (DOF) mobility.

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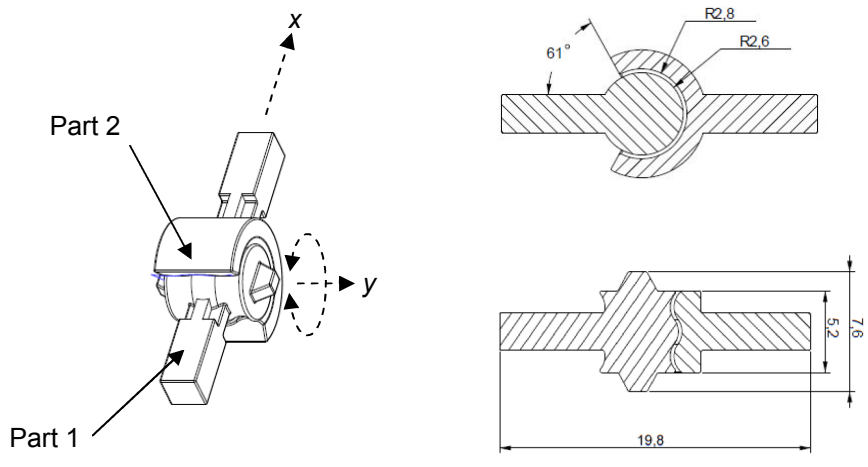
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212 **Fig. 2.** A CAD illustration of the moving joint (all dimensions are in millimetres).

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The in-situ assembly mechanism is achieved through the free-form design of the mating surfaces of the subcomponents that are designed such that they are inseparable throughout the manufacturing process. This design philosophy constrains the relative motions of parts 1 and 2 in all directions, except for the required 120-degree rotational movement around the y -axis. Part 1 is designed as a cylinder with a symmetrical curved surface. A similar curvature is introduced into the inside geometry of the socket of part 2, leaving a space of 200 μm between the mating surfaces of Parts 1 and 2, such that the two components are constrained in all translational and rotational directions except for rotation around the y -direction (figure 2).

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Part 2 is designed such that the C-shape partially surrounds the cylinder of part 1 making them inseparable in the x -or z -directions. The C-shape of part 2 is designed to allow the required a rotation angle of 120° around the y -axis.

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Both the cylinder and socket are attached to two “arms” that would be inserted into the bones during an operation to insert the prosthesis. In a finalized design, the two arms should have a particular design and structure to fulfil this purpose. In this particular case, they were designed as plain square-sectioned geometries for simplicity. The arms are connected to the cylinder and socket by four ribs each.

2.2.2 Fabrication methodology and procedure.

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The mould used in this experiment was designed such that a replaceable steel insert carries the cavity that is filled with the feedstock during each moulding stage. This enables a quick replacement of

232 the insert without the need to replace the whole mould. Throughout this paper, an “insert” will refer to the
 233 replaceable part of the mould that carries the required cavity.

234 The fabrication methodology was planned following the sequential procedure shown in figure 1.
 235 Figure 3 (a to f) shows a schematic illustration of the fabrication sequence.

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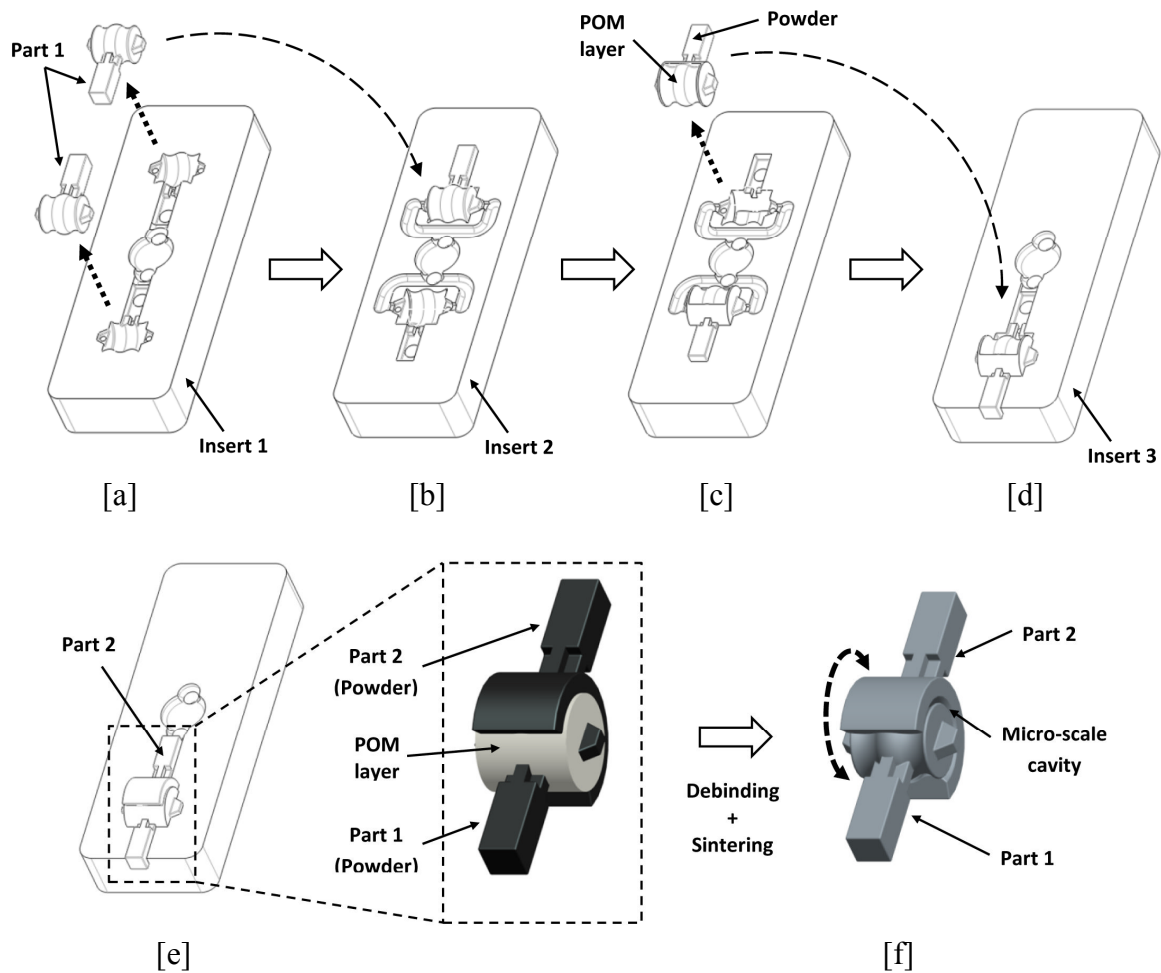
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254 **Fig. 3.** A schematic diagram of the moulding process of a hybrid structure: (a) two pieces of Part 1 are
 255 moulded of 316L and ejected from insert 1. (b) Part 1 pieces are placed in the cavities of insert 2. (c) Part
 256 1 pieces are overmoulded by 200-micron layers of POM and ejected. (d) One overmoulded structure is
 257 placed in the cavity of insert 3 ready for the second overmoulding step. (e) In the second overmoulding
 258 stage, Part 2 is moulded of 316L, resulting in a hybrid structure of Part1, POM layer and Part 2. (f) After
 259 debinding and sintering, Part 2 is movable relative to Part 1.
 260

- 261 • Step 1: Part 1 is moulded by μ PIM using a powder feedstock.
- 262 • Step 2: Part 1 is positioned inside another insert that is machined with extra cavity space for the
 263 polymer layer.

- 264 • Step 3: The sacrificial polymeric layer is micro-overmoulded around part 1 in the defined cavity
- 265 space.
- 266 • Step 4: The resulting compound structure is positioned in a third insert that holds the cavity of part 2.
- 267 • Step 5: Part 2 is overmoulded by μ PIM using a powder feedstock.
- 268 • Step 6: The resulting compound structure is catalytically debound, resulting in the removal of the
- 269 polymeric content, including the sacrificial layer.
- 270 • Step 7: The resulting structure is sintered for full densification.

271 2.2.3 Insert fabrication

272 The procedure shown in figure 3 illustrates that three micro-moulds are required to produce the
 273 ‘green’ compound structure. These moulds were fabricated as replaceable inserts in a single mould body.
 274 The six halves of the inserts were fabricated by micromilling.

275 The machined geometries were characterized by freeform surfaces and high-aspect ratio cavities.
 276 Such complex structures required special micro-cutting tools and special machining sequences,
 277 particularly during the finishing stage, to control the final micro-space between the moving components.
 278 Sintering shrinkage for the selected powder material is typically between 14% and 16%, so oversized
 279 mould cavities were designed and machined taking the final size of the structure into consideration.

280 Inserts were manufactured in hardened steel (Toolox® 33) using a KERN Evo micro-milling
 281 machine. A set of cutting micro-tools was used to cut and finish the inserts, where each cavity is
 282 machined with three roughing stages and one finishing stage. Table 1 summarizes the machining
 283 procedure for the three inserts.

284

285 **Table 1.** Micromilling procedure for the three inserts.

	Mould 1			Mould 2			Mould 3		
	Tool dia. (mm)	Rot. Speed (rpm)	Feed rate (mm/mi n)	Tool dia. (mm)	Rot. Speed (rpm)	Feed rate (mm/mi n)	Tool dia. (mm)	Rot. Speed (rpm)	Feed rate (mm/mi n)
Roughing	1	17600	530	1	17600	530	1	17600	530
Re- roughing 1	0.5	38000	480	0.5	38000	338	0.5	38000	369
Re- roughing 2	0.5	38000	404	0.5	38000	512	0.5	38000	500
Finishing	0.4	41000	420	0.4	41000	420	0.2	41000	26

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288 2.2.4 Sequential micro-overmoulding by μ PIM

289 Powder micro-moulding was used to produce the green hybrid structure following the procedure
290 above. The moulding conditions of both the powder feedstock and the polymer layer are shown in table 2.

291

292 **Table 2.** Moulding conditions for POM and powder/POM.

Material	Melt temperature [°C]	Mould temperature [°C]	Holding pressure [bar]	Injection velocity [mm/s]	Cooling time [s]
POM	190	100	300	250	10
Powder / POM	190	140	300	250	10

293

294 Polymer moulding and powder overmoulding were performed using a Battenfeld Microsystem
295 50 micro-moulding machine. The polymeric layer was moulded of POM (BASF Ultraform[®] W2320 003)
296 with melt flow index of 25 to ensure better filling of micro-cavities; the powder feedstock was composed
297 of a mixture of 316L stainless steel particles with average particle size (d_{50}) of 4 μ m and POM (BASF
298 Catamold[®] 316LS).

299 2.2.5 Catalytic debinding and sintering

300 During debinding, the compound green structures were placed on a loose-powder bed of alumina
301 for two reasons: Firstly, the powder was used to support the two arms of parts 1 and 2. This is because
302 when the two parts become detached from each other after the removal of the polymer, the torque
303 produced by the weight of the two arms might cause the corresponding parts to tilt against each other and
304 touch at some point, which upon sintering could form a permanent joint. Secondly, the powder bed offers
305 a “flexible” substrate that would not restrict the uniform shrinkage of the two parts due to, for example,
306 friction. The loose powder would allow a simultaneous uniform volumetric shrinkage to take place in the
307 two parts, including the gap in-between, without geometrical deformation.

308 Catalytic debinding took place following the BASF technique (Bloemacher and Weinand, 1997)
309 at a dwell temperature of 110°C in high-concentration nitric acid (>98%) at an acid feed of approximately
310 30 ml/h. Debinding takes place following the so-called “shrinking core mechanism”, by which POM is
311 eliminated layer-by-layer from the outside into the core. Nitrogen was used as a purging gas at a flow rate
312 of approximately 500 l/h. The debinding cycle takes approximately 5 to 6 hours.

313 After debinding, the structure was composed of parts 1 and 2 in powder form between which
314 there was a hollow space. At this stage, the two components were technically separate, although they

315 were fixed in place using the powder bed. The resulting ‘brown’ components were taken directly to the
316 sintering oven while on the powder platform.

317 Sintering was conducted following the schedule shown in table 3, with hydrogen as the gaseous
318 environment. The alumina powder bed facilitated the sintering process by holding the components in
319 place and at the same time allowing them to shrink without bringing them to contact during sintering.

320

321 **Table 3.** Typical sintering schedule for Catamold 316L debound structures.

Stage	Schedule
1	From room temperature to 600°C at the rate of 3°C/min.
2	Hold at 600°C for 1 h.
3	From 600°C to 1250°C at the rate of 3°C/min.
4	Hold at 1250°C for 1 h.
5	From 1250°C to 600°C at the rate of 5°C/min.
6	Furnace cooling.

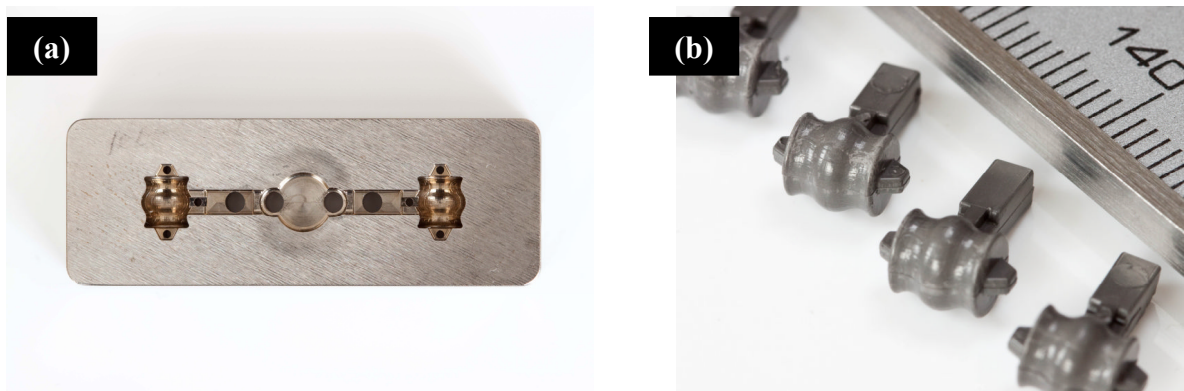
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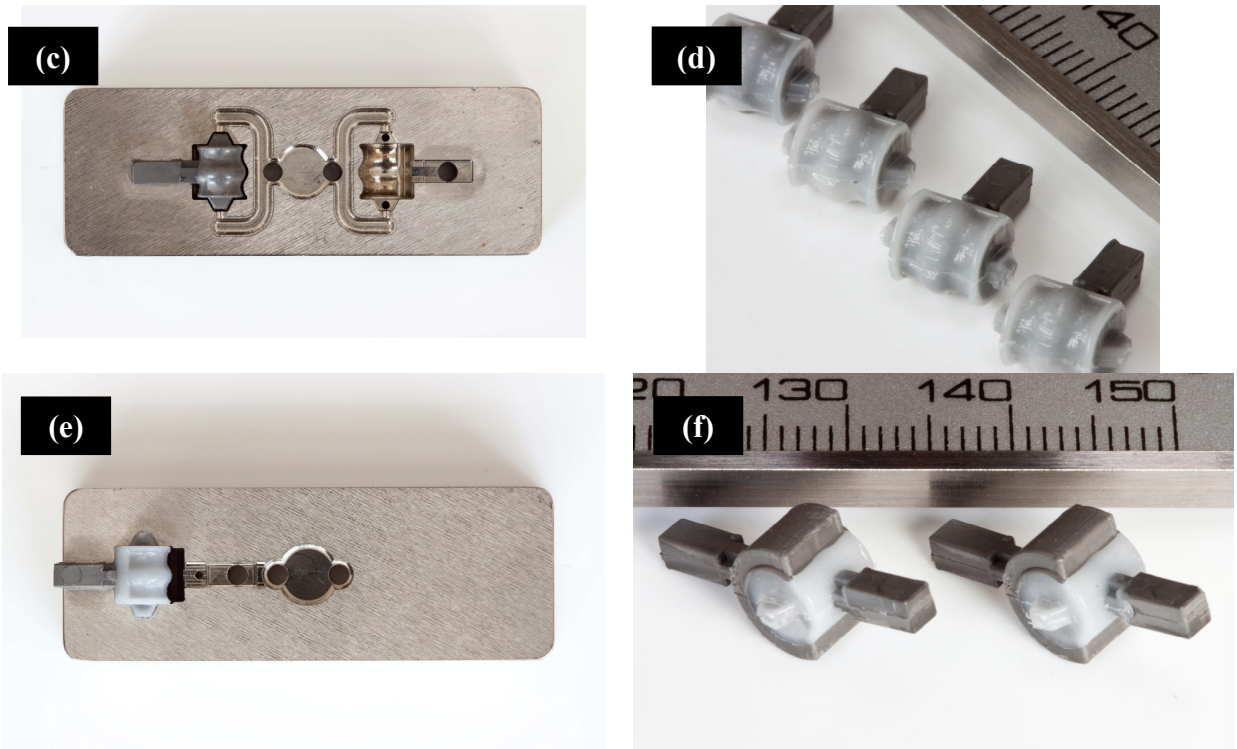
323 The density of the sintered components has been measured using the Archimedes principle, and
324 hardness values have been measured by nanoindentation. Both values have been compared to the
325 theoretical values supplied by the material manufacturer.

326

327 3. Results

328 Figure 4 shows the results of the micro-machining and micro-overmoulding procedure described
329 earlier in section 2.2.2.





330 **Fig. 4.** (a) a twin-cavity insert for part 1 (b) part 1 samples replicated from 316LS feedstock (c) a twin-
 331 cavity insert for POM layer with part 1 sample placed in one cavity for illustration (d) part 1 samples
 332 micro-overmoulded with POM layers (e) an insert for component 2 with the overmoulded part 1 for
 333 illustration (f) samples of the complete hybrid green structure of parts 1 and 2 with the POM layer.
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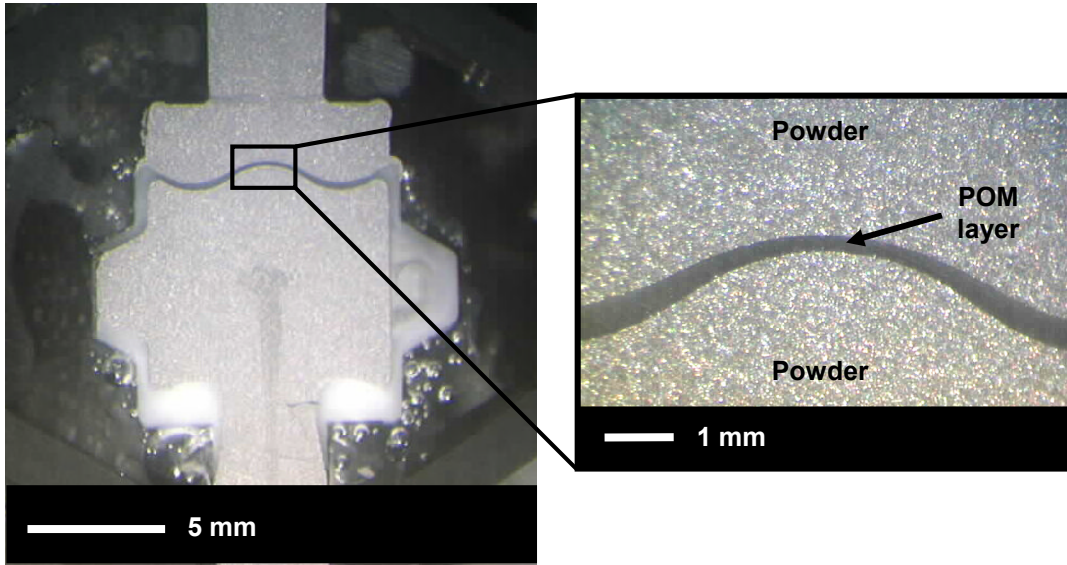
336 Figures 4a and 4b show the mould of part 1 and the replicated green component, respectively.
 337 The micro-moulding of the sacrificial POM layer is shown in figures 4c and 4d, where the former shows
 338 the mould in which part 1 was positioned, and the latter shows part 1 covered with the sacrificial POM
 339 layer where the moving space is eventually required. Figure 4c shows how the mould was designed with
 340 two registration cavities to secure the positioning of part 1 inside the mould whilst the POM layer is being
 341 overmoulded. The overmoulding of part 2 is shown in figures 4e and 4f, where the former shows the third,
 342 and final, mould cavity, and the latter shows the full compound hybrid structure.

343 Figure 5 shows a cross section in the hybrid green structure. The figure shows a symmetric layer
 344 of POM between parts 1 and 2 with variable thickness. Measurements indicate an average thickness of
 345 246 μm at narrowest distance in the middle. The largest distances at the sides have average thicknesses of
 346 367 μm .

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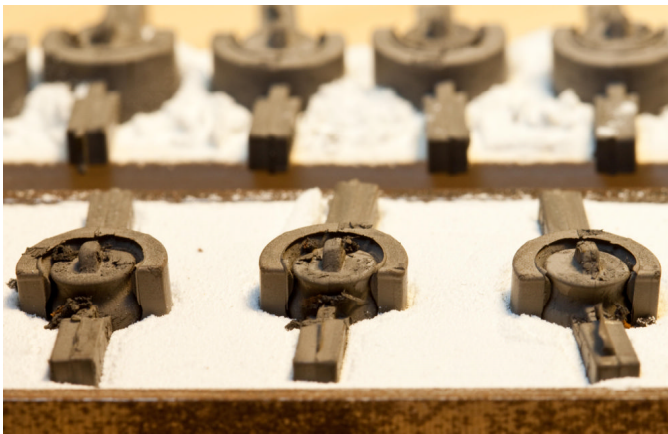
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359 **Fig. 5.** A cross section in a green structure with an enlarged view of the micro-sacrificial layer.

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Figure 6 shows a batch of “brown” structures after catalytic debinding positioned on the powder bed. The figure shows each structure consisting of two distinct components with a cavity in between with no visible traces of polymeric material.



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365 **Fig. 6.** Brown structures on a powder bed after catalytic debinding.

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Figure 7 shows the final structures after sintering with a movable joint produced between the sub-components.



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371 **Fig. 7.** Sintered structures with movable joints.

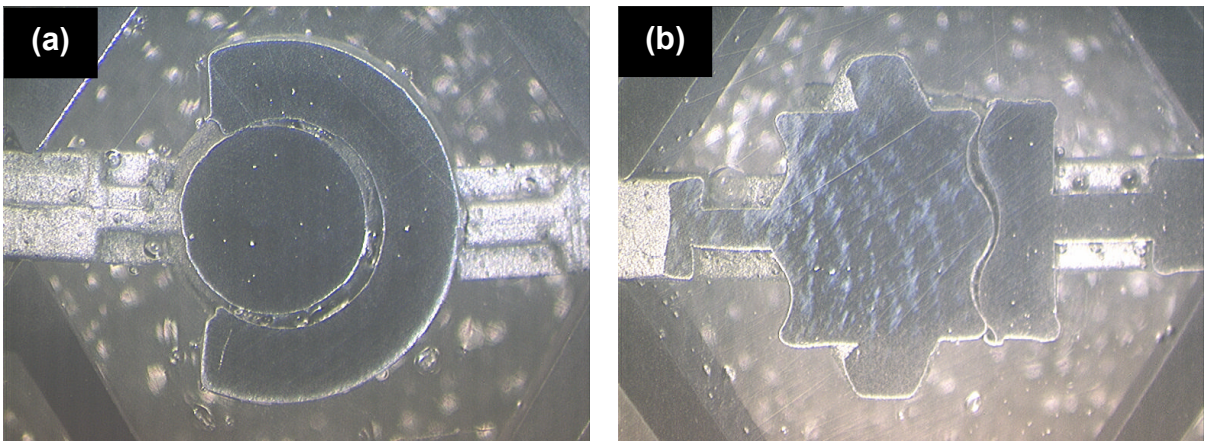
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373 Figure 8 shows microscopy images of cross sections in the sintered components. Figure 8a is a

374 cross section normal to the rotation axis, whilst figure 8b is a cross section parallel to the registration

375 features. The images show the micro-cavity between the two subcomponents.

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Fig. 8. Cross sections in the sintered structure (a) normal to the rotation axis and (b) parallel to the registration features.

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Measurements were taken at different points close to the middle of the curved cavity and an average distance of approximately 218 μm was measured. The results illustrated in figures 7 and 8 show that the presented manufacturing technique is viable for producing micro-scale movable interfaces. The micro-overmoulding sequence in figure 4 shows that it is feasible to micro-mould dimensionally

385 controlled sacrificial geometries between powder-based components. The following discussion addresses
386 how the proposed process chain has addresses the five challenges highlighted in section 1.

387 Table 4 shows the density measurements for six samples of the sintered components. The density
388 is also presented as a percentage of the theoretical density specified by the material datasheet (7.9 g/cm^3).
389

390 **Table 4.** Density measurements of six sintered samples

No.	Density [g/cm^3]	% theoretical
1	6.577	83
2	6.533	83
3	6.670	84
4	6.548	83
5	6.716	85
6	6.651	84
Av.	6.616	83.7

391

392 Table 5 presents the results of Vickers hardness values obtained by nanoindentation
393 measurements of five samples. The measurements were taken in two locations with 200-gram load: (a) on
394 the circular section of part 1 and (b) on the arm section of part 2.

395

396 **Table 5.** Micro-hardness measurements of five samples in two locations.

No.	Part 1 hardness [HV]	Part 2 hardness [HV]
1	121	132
2	123	122
3	124	99
4	119	132
5	124	135
Av.	122.2	124

397

398 **4. Discussion**

399 In light of the results of section 3, this section evaluates how the proposed methodology
400 addressed the processing challenges of meso- and micro-scale joints highlighted in the introduction.

401 With regard to the geometrical challenge, the results of figure 4 show that the process is viable in
402 two aspects. Firstly, the micro-overmoulding procedure was performed for truly three-dimensional
403 geometries with free-form surfaces, and the images of the moulded components in figure 4 (b, d and f)
404 show good replication fidelity. Secondly, it was suspected that using the same polymer (POM) for both
405 the powder matrix and the core might increase the likeliness of deformation at the interface due to the
406 similar thermal properties. However, this was not observed during processing, and the cross section in

407 figure 5 shows a hybrid green component with good shape retention and clear boundaries between the
408 powder shell and the polymer micro-layer.

409 With regard to the material variety challenge, the presented process is applicable to any powder-
410 base mouldable feedstock. Commercially available feedstock covers a wide range of metals and ceramics
411 with different mechanical, thermal and biomedical properties. In addition, powder feedstock with
412 relatively small average particle sizes (in the order of few micrometres for metals and a few hundred
413 nanometres for ceramics) is available, which enables the replication of meso- and micro-scale
414 components. The presented process, therefore, offers a true shift from conventional materials associated
415 with microfabrication such as silicon and SU8.

416 With regard to the assembly challenge, figures 5 and 6 show that the two parts are readily
417 assembled and movable relative to each other. This was achieved in-situ by combining a design solution
418 with a processing solution. The former was concerned with designing the internal geometries of both
419 parts such that they are inseparable once a cavity is created between them. The latter solution was
420 concerned with planning the processing steps such that alignment is readily achieved during the
421 overmoulding stages by using registration marks and positioning constraints in the mould structure. This
422 manufacturing strategy enables in-situ assembly, alignment and motion already after the debinding stage,
423 The sintering stage was just to treat the components into the final density.

424 With regards to powder-based fabrication challenges, figure 6 of the debound components shows
425 that the manufacturing principle is viable for producing sacrificial micro-cavities for powder-based
426 moving joints. Unlike previous work reported in the literature that relied on controlling shrinkage rates to
427 produce a movable interface, this approach overcomes this challenge by creating the interface through a
428 micro-moulded sacrificial layer that precisely defines the final clearance between the moving components.

429 The images show that the POM micro-layer was totally consumed whilst the overall component
430 retains its geometry. Other than a few defects inherited from the moulding process, such as the broken-
431 gate remains or ejection-pin marks, the debinding process did not distort the geometrical integrity of the
432 structure.

433 The cross sections of the sintered component illustrated in figure 8 show the cavity maintained in
434 the structure. No visible signs of deterioration have been detected, and shape retention appears of high
435 quality. Again no signs of particular problems related to cavity encapsulation were observed. The

436 measured cavity was approximately 218 μm , which corresponds to a linear shrinkage of approximately
437 11% from the 246- μm POM layer. This shrinkage is slightly lower than the 14% specified by the powder
438 feedstock datasheet, which implies the need for better process control during sintering.

439 Density measurements reported in Table 4 show that the component density is about 84% of the
440 theoretical density specified by the material manufacturer. This could be explained by the fact that
441 sintering took place at 1250°C (maximum allowed by the equipment available), which is 100 degrees
442 lower than the recommended 1360 °C sintering temperature recommended by the material supplier. The
443 lower temperature was not sufficient to reach full densification. This also explains the lower value of
444 shrinkage discussed earlier.

445 Hardness values reported in Table 5 shows that average values for Part 1 (122 HV) and Part 2
446 (124 HV) are close to the theoretical value specified by the material datasheet (120 HV). The variation in
447 the hardness measurements reported in Table 5 could be due to error in measurements due to the small
448 sizes of the samples.

449 With regard to mass manufacturability, micro-moulding of polymers is already being
450 implemented on an industrial scale, and micro-moulding of metals has the same potential. The moulding
451 processes themselves are relatively short (tens of seconds), and the longest time was used to position the
452 components manually into the inserts at each overmoulding stage. Automating the insert loading process
453 would overcome this obstacle on a mass-manufacturing scale.

454 Figures 7 and 8 indicate the feasibility of the presented process chain in producing metallic
455 movable joints with micro-scale interface by μPIM after addressing the main five challenges highlighted
456 in the introduction. It should be noted, however, that the fabrication strategy has a number of limitations
457 that need to be addressed. One limitation is that each stage of the process is effectively a micro-moulding
458 process, which requires the geometry design to be demouldable from a two-half mould. This limits the
459 producible geometries relative to, for example, SLS. In addition, all dimensions of the powder
460 components are limited by the particle size, as it is recommended that the minimum feature size should be
461 at least 10-20 times the particle size, as recommended by German (2009) and Piotter et al. (2005).

462 It should also be noted that the dimensional accuracy of the replicated components can be as
463 good as the corresponding mould dimensions themselves. Although the designed distance between the
464 moving components was 235 μm , the actual moulded POM layer was 246 μm at its narrowest point due

465 to machining variations. This resulted in a post-sintered cavity distance of 218 μm with an extra 9%
466 increase in cavity size.

467 Future work will focus on overcoming such limitations by improved geometry design and
468 process control. Research will also focus on implementing the process for smaller structure size and a
469 variety of powder materials.

470

471 **5. Conclusion**

472 This paper presents a processing strategy for creating micro-scale cavities between moving
473 components. The proposed process route combines the capabilities of powder micro-moulding, micro-
474 overmoulding, catalytic debinding and sintering. An articulated structure with a single degree of freedom
475 was used as a demonstrator for the technology. The produced components showed that the process routes
476 are feasible and no serious challenges were encountered, except for the need to investigate other mould-
477 fabrication methods and optimise process conditions for dimensional control. Density measurements
478 showed that the components were approximately 84% of the theoretical density, which is due to sintering
479 taking place below the recommended temperature. Hardness measurements showed average values close
480 to the theoretical values. Further experimentation is required to assess the feasibility of the process for
481 smaller, micro-scale dimensions and for different powder-based materials.

482

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485

486 **References**

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